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1 Maximum Voluntary Isometric Torque Production for Task specific and Single-
2 joint Muscle groups and their Relation to Peak Power Output in Sprint Cycling.

3

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23 Cycling

24

25 **ABSTRACT**

26 From a cycling paradigm, little has been done to understand the relationships between maximal
27 isometric strength of different single joint lower body muscle groups and their relation with, and
28 ability to predict PPO and how they compare to an isometric cycling specific task. The aim of this
29 study was to establish relationships between maximal voluntary torque production from isometric
30 single-joint and cycling specific tasks and assess their ability to predict PPO. Twenty male trained
31 cyclists participated in this study. Peak torque was measured by performing maximum voluntary
32 contractions (MVC) of knee extensors, knee flexors, dorsi flexors and hip extensors whilst
33 instrumented cranks measured isometric peak torque from MVC when participants were in their
34 cycling specific position (ISOCYC). A stepwise regression showed that peak torque of the knee
35 extensors was the only significant predictor of PPO when using SJD and accounted for 47% of the
36 variance. However, when compared to ISOCYC, the only significant predictor of PPO was ISOCYC,
37 which accounted for 77% of the variance. This suggests that peak torque of the knee extensors was
38 the best single-joint predictor of PPO in sprint cycling. Furthermore, a stronger prediction can be
39 made from a task specific isometric task.

40

41 INTRODUCTION

42 First described by Hill in 1938, mechanical power produced by muscle is the consequence of force
43 production and shortening velocity (Hill, 1938). These two variables share a hyperbolic, inverse
44 relationship with peak concentric mechanical power being achieved at approximately a third of
45 maximal shortening velocity and maximum concentric force (Edman, 1979). From an applied
46 perspective, maximal power output acts as one of the main physiological determinants and predictors
47 of performance in sports such as running (Bundle and Weyand, 2012; Weyand et al., 2006), rowing
48 (Ingham et al., 2002) and jumping (Ferretti et al., 1994; Grassi et al., 1991). Similarly, from a sprint
49 cycling perspective, mechanical peak power output (PPO) at the crank level acts as a primary
50 physiological determinant of performance. (Dorel et al., 2005; Martin et al., 2006, 2007)

51 Torque (cycling equivalent of force) and cadence (cycling equivalent of shortening velocity) are
52 inversely related, however, unlike the descriptions of Hill, they are linearly, not hyperbolically related
53 (Driss et al., 2002; Driss and Vandewalle, 2013; Gardner et al., 2007; Jaafar et al., 2015; Martin et al.,
54 1997). As such, PPO is achieved at approximately half of the maximum extrapolated torque (T_{\max})
55 and maximum extrapolated cadence (C_{\max}) (Dorel et al., 2005; Gardner et al., 2007), which is reported
56 to occur ~120 rpm (Samozino et al., 2007); however, conceptually an increase in T_{\max} and/or C_{\max}
57 could result in an increased PPO, and by inference, performance.

58 To date, evidence to suggest what physiologically underpins PPO and sprint cycling performance is
59 limited to thigh volume (Dorel et al., 2005). Other studies have used non-sporting populations to
60 significantly correlate fat free mass (Duché et al., 2002) and isometric quadriceps strength (Driss et
61 al., 2002). Despite Driss et al. (2002) and colleagues reporting strong correlations between maximal
62 voluntary contractions (MVCs) during isometric knee extension in relation to both T_{\max} ($r = 0.73$) and
63 PPO ($r = 0.75$) in sprint cycling, there seems to be a plethora of data associating isometric MVCs with
64 dynamic performance providing varied results. Typically correlations range between 0.3 and 0.6,
65 whilst perhaps unsurprisingly, much stronger relationships have been observed ($r = 0.76 - 0.97$) when
66 the isometric MVC has a great degree of specificity to the dynamic performance task (for review see
67 (Wilson and Murphy, 1996)). Typically, non-specific tasks that isolate single-joint muscle groups

78 have been used to determine performance, but these are of limited use given the performance action is
79 often very different to the surrogate measure, therefore a task specific measure would be conceptually
80 better (Wilson and Murphy, 1996). This is exemplified in using maximum isometric force in a bench
81 press test to predict performance in shotput throwers where a poor relationship was observed ($r =$
82 0.22) as the isometric task lacked specificity to the ‘dynamic’ performance measure. Notwithstanding,
83 maximum isometric force was strongly correlated with (dynamic) bench press 1RM ($r = 0.78$) due to
84 the performance and isometric task being very similar (Murphy et al., 1994), which further illustrates
85 the issue of task specificity.

86 The limitation of the study carried out by Driss et al. (2002) was that it was limited to the knee
87 extensors only, whereas sprint cycling is a compound movement and uses all major muscle groups in
88 the lower limbs to produce impulse (Dorel et al., 2012). Consequently, it is important to investigate,
89 and therefore gain, greater understandings of whether other muscle groups (beyond knee extensors)
90 contribute to PPO and sprint cycling performance.

91 The implications of this study can be used to provide athletes, coaches and practitioners an evidence-
92 based strength testing battery which can be used to monitor and predict sprint cycling performance.
93 Further, investigating a cycling specific isometric task will in comparison to single joint will give a
94 better idea to see if non-specific cycling strength vs. cycling specific cycling strength in relation to
95 performance.

96 The aims of this study were two-fold. Firstly, we examined the yet untested relationship of maximal
97 strength of the major lower body cycling muscles using isometric single-joint dynamometry and
98 whether any can be used to predict PPO. Secondly, we assessed whether an isometric cycling-specific
99 task would be a better predictor of sprint cycling performance than isolated isometric single-joint
100 muscle group tasks.

91 **METHODS**

92 **Participants**

93 Twenty male cyclists volunteered to take part in the study (mean \pm SD age, 27 ± 5 yr; stature, $183.1 \pm$
94 8.4 cm; mass, 84.5 ± 11.1 kg). Cycling training experience and rider category varied throughout the
95 participants, but all were engaged between 5-24 h of training per week and were regularly competing
96 in various disciplines from sprint track to road endurance cycling from British Cycling's 'Category 3'
97 up to the 'Elite category' national level riders. The cyclists were free from injury as assessed by a
98 health screening questionnaire. Following institutional ethics committee approval, cyclists provided
99 written, informed consent prior to any experimental procedures.

100 **Study Overview**

101 Participants attended two familiarisation sessions prior to the two experimental sessions. All lab
102 sessions were identical whereby participants completed the same protocol on each lab visit. Lab visits
103 were separated by at least 1 and not more than 7 d. Cyclists were asked to report to the laboratory in a
104 hydrated state and to avoid caffeine and food for 3 h prior to testing and to avoid intense exercise in
105 the 24 h before each session. Firstly, the participants performed isolated, isometric, single-joint MVCs
106 with four different muscle groups (knee extensors, knee flexors, hip extensors and plantar flexion) on
107 a dynamometer. Subsequently, after 15 minutes of passive rest, participants performed a series of
108 cycling-specific, multi-joint isometric MVCs on an instrumented, custom made cycling ergometer.
109 Lastly, a maximum isokinetic power-cadence protocol was performed to measure PPO.

110 **Isometric Dynamometry**

111 Each laboratory session started with participants performing isometric MVCs on a calibrated
112 dynamometer (Biodex, System 4 Pro, New York, USA). Participants performed MVCs on four
113 different muscle groups on each leg (always starting on the right side) before proceeding to the next
114 muscle group, in the following order: plantar extensors (calf), hip extensors (gluteal), knee extensors
115 (quadriceps) and knee flexors (hamstrings).

116 After five, 3 s sub-maximal contractions of progressing intensity, participants performed three, 3 s
117 MVCs which were separated by 60 s of rest. The subjects were asked to maximally contract "as hard
118 as possible" to ensure that maximal torque was achieved within the 3s. The isometric joint angles

119 were fixed at what has previously been reported as optimal torque producing angles: hip (45°), knee
120 (70° in extension and 50° in flexion) and ankle (0°) (Dorel et al., 2012; Ericson, 1986; Rouffet and
121 Hautier, 2008). Specific dynamometer positions were recorded for each participant during the first
122 familiarisation session and replicated thereafter. Between each set of MVCs (between each leg and
123 muscle group), participants were given 5 minutes passive rest.

124 **Cycling Specific Isometric Protocol (ISOCYC)**

125 Participants performed the multi-joint cycling specific isometric (ISOCYC) MVCs on a custom made
126 cycling ergometer (BAE Systems, London, UK), which was modified to allow for isometric efforts by
127 attaching a clamp to the flywheel. The ergometer was set up to replicate the participants' cycling
128 position whilst using their own cycling shoes and pedals. The participants performed the ISOCYC
129 MVCs in the saddle and were instructed to remain seated throughout. To further ensure that they
130 remained seated, they were strapped into the saddle using a webbing seatbelt, secured and tightened
131 around their waist and ergometer whilst their forearms were positioned on the crossbar of the
132 handlebars. The drive-side (right) crank arm was positioned at 90° from top, dead centre (TDC) using
133 an inclinometer. As with the dynamometer, the participants were given three sub-maximal efforts at
134 what they perceived at 60%, 70% and 80% of their perceived MVC. Prior to performing the ISOCYC
135 efforts, participants were reminded to 'try to pedal the cranks forward as hard as possible using both
136 legs' (i.e., the right leg pushing down and the left leg pulling up, simultaneously). Following a 3 s
137 countdown, participants performed a 3 s MVC, which was performed 3 times with 60 s rests in
138 between efforts. After 5 minutes passive rest, the process was then repeated with the only difference
139 being the drive side (right) and non-drive side (left) crank positions being reversed. The ergometer
140 was fitted with instrumented cranks (170 mm) that following calibration, measured cumulative, as
141 well as individual, right and left crank arm torque production (Factor Cranks, BF1 Systems, Diss, UK)
142 at a sampling rate of 200 Hz.

143 **Isokinetic Peak Power Output Protocol**

144 Prior to performing the maximal isokinetic efforts to determine PPO, participants undertook a
145 standard 10-minute warm-up of submaximal cycling at a self-selected intensity (between 100-150 W)
146 and cadence (between 80-90 RPM). For the maximal isokinetic efforts, participants performed 4 s
147 sprints at 60, 110, 120, 130 and 180 RPM. Cadences were randomised for all laboratory sessions
148 (www.random.org). Prior to each effort, the motor was brought up to the desired velocity and
149 participants were instructed to pedal below the pre-set cadence and reminded to ‘attack the effort as
150 fast and as hard as possible’ once the effort began. The investigator gave a 3 s countdown and the
151 participants performed a 4 s maximal effort against the set cadence. A period of 3 minutes passive rest
152 was given between each isokinetic sprint. As with the ISOCYC, participants used their own cycling
153 shoes and pedals and performed the PPO protocol on ergometer, which was identically set-up to their
154 racing positions. All efforts were performed in the saddle with each cyclist using the ‘drop’
155 handlebars.

156 **Data Processing**

157 Torque from the dynamometer was sampled (2,000 Hz) and fed directly into a data acquisition system
158 (Micro 1401, CED, Cambridge, United Kingdom) and the accompanying PC utilizing Spike2
159 software (CED, Cambridge, United Kingdom). Of the three MVCs, the highest peak torque value
160 (from the isometric dynamometry) for each individual muscle group was recorded. As the
161 performance task (sprint cycling) uses both limbs, peak torque values were averaged for both right
162 and left muscle groups for each experimental session and then averaged again over both experimental
163 sessions. Likewise, peak torque values from right and left cranks in all ISOCYC efforts were
164 extracted and averaged for both sessions and then averaged between sessions.

165 For both ISOCYC and PPO efforts, data was being recorded wirelessly on to an electronic measuring
166 system (BF1 Systems, Diss, United Kingdom). Subsequent to each lab session, the raw data was
167 exported into Spike2, where power and cadence was calculated using custom made scripts. For the
168 isokinetic PPO sprints, the first three full revolutions (from TDC to TDC) of each effort at the pre-
169 determined cadence were recorded and analysed; the revolution with the highest mean torque (and

170 therefore, power) was used. For each participant, the revolution analysed for each cadence was
171 averaged between sessions. Then, the five power outputs at each pre-determined cadences, a quadratic
172 regression power-cadence relationship was plotted and PPO was interpolated at the apex of the curve.

173 **Statistical Analysis**

174 The relationship between PPO and peak torques for different muscle groups in isometric
175 dynamometry MVCs and the ISOCYC were calculated by using a Pearson's product moment
176 correlation. Pearson's correlation coefficients were defined as previously described by Buchheit and
177 colleagues: trivial (0.0), small (0.1), moderate (0.3), strong (0.5), very strong (0.7), nearly perfect
178 (0.9), and perfect (1.0) (Buchheit et al., 2010). Any correlation greater than $r = 0.50$ was used in a
179 step-wise linear regression to predict PPO from peak torque values from isometric dynamometry of
180 relevant muscle groups. If any were seen as significant predictors, they were placed into another step-
181 wise linear regression against ISOCYC to determine whether a more task specific or a non-skilled
182 task best predicts PPO. All statistics was performed on SPSS (IBM Corp., Armonk, N.Y., USA) and
183 reported as mean (SD) unless otherwise stated.

184 **RESULTS**

185 Average mechanical PPO was measured at 1197 ± 215 W (Figure 1). In relation to PPO, maximum
186 isometric strength of the knee extensors showed a very strong relationship ($r = 0.71$; $p < 0.01$). Strong
187 relationships were also observed between the knee flexors ($r = 0.53$; $p = 0.02$), the hip extensors ($r =$
188 0.56 ; $p = 0.01$) and PPO with a trivial, non-significant relationship between ankle extensors and PPO
189 ($r = -0.03$; $p = 0.89$). The relationship between PPO and ISOCYC (Figure 2) had a very strong
190 relationship ($r = 0.87$; $p < 0.01$).

191 All isometric dynamometry muscle groups that were assessed (apart from the plantar extensors) were
192 entered into a step-wise regression model and significantly predicted PPO ($F_{(3, 19)} = 16.06$, $p = 0.001$,
193 $R^2 = 0.47$). However, only peak torque from isometric knee extension contributed significantly to the
194 prediction, which accounted for 47% of the variation in PPO ($p = 0.001$). Knee flexion ($p = 0.460$)
195 and hip extension ($p = 0.507$) did not contribute meaningfully to the prediction. Accordingly, peak

196 torques of knee extensors and ISOCYC were put into a subsequent step-wise regression model and
197 PPO was significantly predicted ($F_{(2, 19)} = 23.55$, $p < 0.001$, $R^2 = 0.77$). Only peak isometric torque
198 from ISOCYC added statistical significance to the prediction, which accounted for 77% of the
199 variation ($p = 0.001$). Knee extension did not contribute significantly to the relationship ($p = 0.389$).

200 **DISCUSSION**

201 The purpose of this study was two-fold. Firstly, to establish whether maximal torque produced from
202 single joint isometric dynamometry can significantly predict PPO in sprint cycling. Secondly, how
203 single joint isometric dynamometry compares to a cycling specific isometric task in predicting PPO.
204 With respect to the first aim, of all the major lower body muscle groups that were assessed using
205 isometric single joint MVC, peak torque produced by the knee extensors was shown to be a
206 significant predictor of PPO. However, with respect to the second aim, when peak torque from the
207 knee extensors was compared to peak torque produced by ISOCYC, it was the cycling specific
208 measure of maximal strength that was shown to be the only significant predictor of PPO.

209 With ISOCYC being the best predictor of PPO and therefore, the potential to predict sprint cycling
210 performance, it builds on the growing body of evidence that task specific isometric contractions are a
211 better predictor of performance than non-skilled, single-joint tasks, like isometric dynamometry. The
212 ISOCYC is easy to perform, is a more familiar task to trained cyclists and in comparison to
213 dynamometry is significantly cheaper. Furthermore, should the instrumented cranks be on their own
214 bike, it can be performed almost anywhere. The disadvantage of using an isometric compound
215 movement, like ISOCYC, to an isolated single joint MVC, is that it does not provide sufficient
216 information to ascertain which muscle groups are responsible for any changes that may be observed.

217 Previously, instrumented cranks have been able to provide power-cadence (and torque-cadence)
218 relationships as an accurate means to model cycling performance in the laboratory which is reflected
219 in field performances (Gardner et al., 2007). However, though this may be thought of as a more
220 ecologically valid task, it involves a large technical/biomechanical component that makes it hard to
221 quantify true physiological changes in strength of muscle group(s). Isometric tasks (single-joint

222 dynamometry (in this case, knee extensor assessment) can provide valuable information of strength
223 changes in targeted muscle groups. This means that it can act as an abstract measure of strength that is
224 far removed from the task, can be monitored by coaches and practitioners to provide information on
225 meaningful changes in physiological strength relative to a key performance measure as well as
226 provide valuable feedback on the efficacy of previous training or indeed inform the prescription and
227 monitoring of future training programming.

228 The findings from the single joint dynamometry concur with previous work (Driss et al., 2002) that
229 showed a similar, strong relationship between isometric MVC of the knee extensor and PPO. The hip
230 extensors and knee flexors displayed large and significant relationships to PPO and but they did not
231 significantly add to the regression model that already included the knee extensors. No relationship
232 between maximal plantar flexor strength with PPO was observed which is contrary to the high
233 muscle activation levels of the plantar flexors during maximal sprint cycling (Dorel et al., 2012). A
234 possible explanation for this finding could either that plantar flexor strength may be more cycling/task
235 specific rather than a general, non-specific, abstract strength measure and/or may provide some
236 evidence that the planar flexors are involved in the transfer of mechanical energy from the proximal
237 muscles to the crank (Raasch et al., 1997).

238 A plausible suggestion for why knee extensors are the only significant single joint predictors of PPO
239 could be because the superficial mono-articular muscles of the quadriceps (i.e. VM and VL) are
240 maximally activated when peak torque is achieved around the crank cycle (Dorel et al., 2012). Thus,
241 stronger knee extensors are critical for high instantaneous torque and therefore, PPO. Nevertheless,
242 irrespective of why the knee extensors are the best predictor of PPO, peak torque from ISOCYC
243 MVCs provides a task specific, less time consuming, cheaper method to predict PPO that is easy to
244 administer and can be used by athletes, coaches and practitioners to monitor changes in PPO and
245 therefore make some inference about performance.

246 There are limitations to this study that should be mentioned. Firstly, it is recommended that at least 50
247 participants are used when employing a multiple linear regression in comparison to the 20 used in this

248 study (Green, 1991). In addition, not all the major muscle groups were assessed. Two major lower
249 body muscle groups: hip flexors and dorsiflexors were not assessed which have been shown to be
250 maximally active during sprint cycling (Dorel et al., 2012) and no upper body measures which have
251 been shown to contribute to high intensity cycling even though it is sub-maximal (Grant et al., 2015).

252 In conclusion, of all the major lower body muscle groups, peak torque in the knee extensors from
253 isometric dynamometry was the best predictor of peak power output in sprint cycling. Moreover, our
254 data show that a stronger prediction of sprint cycling performance can be made from a measure of
255 maximal torque that is performed in an isometric cycling specific task to indirectly assess PPO. This
256 provides a cheaper, easier and more applicable method for athletes, coaches and practitioners to
257 monitor surrogate measures of sprint cycling performance.

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261 **CONFLICTS OF INTEREST**

262 The authors do not have any conflicts of interest.

263 **REFERENCES**

- 264 Buchheit, M., Mendez-Villanueva, A., Simpson, B.M., Bourdon, P.C., 2010. Match running
265 performance and fitness in youth soccer. *Int. J. Sports Med.* 31, 818–825. doi:10.1055/s-0030-
266 1262838
- 267 Bundle, M.W., Weyand, P.G., 2012. Sprint exercise performance: does metabolic power matter?
268 *Exerc. Sport Sci. Rev.* 40, 174–182. doi:10.1097/JES.0b013e318258e1c1
- 269 Dorel, S., Guilhem, G., Couturier, A., Hug, F., 2012. Adjustment of muscle coordination during an
270 all-out sprint cycling task. *Med. Sci. Sports Exerc.* 44, 2154–2164.
271 doi:10.1249/MSS.0b013e3182625423
- 272 Dorel, S., Hautier, C.A., Rambaud, O., Rouffet, D., Van Praagh, E., Lacour, J.-R., Bourdin, M., 2005.
273 Torque and power-velocity relationships in cycling: relevance to track sprint performance in
274 world-class cyclists. *Int. J. Sports Med.* 26, 739–746. doi:10.1055/s-2004-830493
- 275 Driss, T., Vandewalle, H., 2013. The measurement of maximal (anaerobic) power output on a cycle
276 ergometer: a critical review. *BioMed Res. Int.* 2013, 589361. doi:10.1155/2013/589361
- 277 Driss, T., Vandewalle, H., Le Chevalier, J.-M., Monod, H., 2002. Force-velocity relationship on a
278 cycle ergometer and knee-extensor strength indices. *Can. J. Appl. Physiol. Rev. Can. Physiol.*
279 *Appliquée* 27, 250–262.

280 Duché, P., Ducher, G., Lazzer, S., Doré, E., Tailhardat, M., Bedu, M., 2002. Peak power in obese and
281 nonobese adolescents: effects of gender and braking force. *Med. Sci. Sports Exerc.* 34, 2072–
282 2078. doi:10.1249/01.MSS.0000039305.73223.2E

283 Edman, K.A., 1979. The velocity of unloaded shortening and its relation to sarcomere length and
284 isometric force in vertebrate muscle fibres. *J. Physiol.* 291, 143–159.

285 Ericson, M., 1986. On the biomechanics of cycling. A study of joint and muscle load during exercise
286 on the bicycle ergometer. *Scand. J. Rehabil. Med. Suppl.* 16, 1–43.

287 Ferretti, G., Narici, M.V., Binzoni, T., Gariod, L., Le Bas, J.F., Reutenauer, H., Cerretelli, P., 1994.
288 Determinants of peak muscle power: effects of age and physical conditioning. *Eur. J. Appl.*
289 *Physiol.* 68, 111–115.

290 Gardner, A.S., Martin, J.C., Martin, D.T., Barras, M., Jenkins, D.G., 2007. Maximal torque- and
291 power-pedaling rate relationships for elite sprint cyclists in laboratory and field tests. *Eur. J.*
292 *Appl. Physiol.* 101, 287–292. doi:10.1007/s00421-007-0498-4

293 Grant, M.C., Watson, H., Baker, J.S., 2015. Assessment of the upper body contribution to multiple-
294 sprint cycling in men and women. *Clin. Physiol. Funct. Imaging* 35, 258–266.
295 doi:10.1111/cpf.12159

296 Grassi, B., Cerretelli, P., Narici, M.V., Marconi, C., 1991. Peak anaerobic power in master athletes.
297 *Eur. J. Appl. Physiol.* 62, 394–399.

298 Green, S.B., 1991. How Many Subjects Does It Take To Do A Regression Analysis. *Multivar. Behav.*
299 *Res.* 26, 499–510. doi:10.1207/s15327906mbr2603_7

300 Hill, A.V., 1938. The Heat of Shortening and the Dynamic Constants of Muscle. *Proc. R. Soc. B Biol.*
301 *Sci.* 126, 136–195. doi:10.1098/rspb.1938.0050

302 Ingham, S.A., Whyte, G.P., Jones, K., Nevill, A.M., 2002. Determinants of 2,000 m rowing ergometer
303 performance in elite rowers. *Eur. J. Appl. Physiol.* 88, 243–246. doi:10.1007/s00421-002-
304 0699-9

305 Jaafar, H., Attiogbé, E., Rouis, M., Vandewalle, H., Driss, T., 2015. Reliability of Force-Velocity
306 Tests in Cycling and Cranking Exercises in Men and Women. *BioMed Res. Int.* 2015,
307 954780. doi:10.1155/2015/954780

308 Martin, J.C., Davidson, C.J., Pardyjak, E.R., 2007. Understanding sprint-cycling performance: the
309 integration of muscle power, resistance, and modeling. *Int. J. Sports Physiol. Perform.* 2, 5–
310 21.

311 Martin, J.C., Gardner, A.S., Barras, M., Martin, D.T., 2006. Modeling sprint cycling using field-
312 derived parameters and forward integration. *Med. Sci. Sports Exerc.* 38, 592–597.
313 doi:10.1249/01.mss.0000193560.34022.04

314 Martin, J.C., Wagner, B.M., Coyle, E.F., 1997. Inertial-load method determines maximal cycling
315 power in a single exercise bout. *Med. Sci. Sports Exerc.* 29, 1505–1512.

316 Murphy, A.J., Wilson, G.J., Pryor, J.F., 1994. Use of the iso-inertial force mass relationship in the
317 prediction of dynamic human performance. *Eur. J. Appl. Physiol.* 69, 250–257.

318 Raasch, C.C., Zajac, F.E., Ma, B., Levine, W.S., 1997. Muscle coordination of maximum-speed
319 pedaling. *J. Biomech.* 30, 595–602.

320 Rouffet, D.M., Hautier, C.A., 2008. EMG normalization to study muscle activation in cycling. *J.*
321 *Electromyogr. Kinesiol. Off. J. Int. Soc. Electrophysiol. Kinesiol.* 18, 866–878.
322 doi:10.1016/j.jelekin.2007.03.008

323 Samozino, P., Horvais, N., Hintzy, F., 2007. Why does power output decrease at high pedaling rates
324 during sprint cycling? *Med. Sci. Sports Exerc.* 39, 680–687.
325 doi:10.1249/MSS.0b013e3180315246

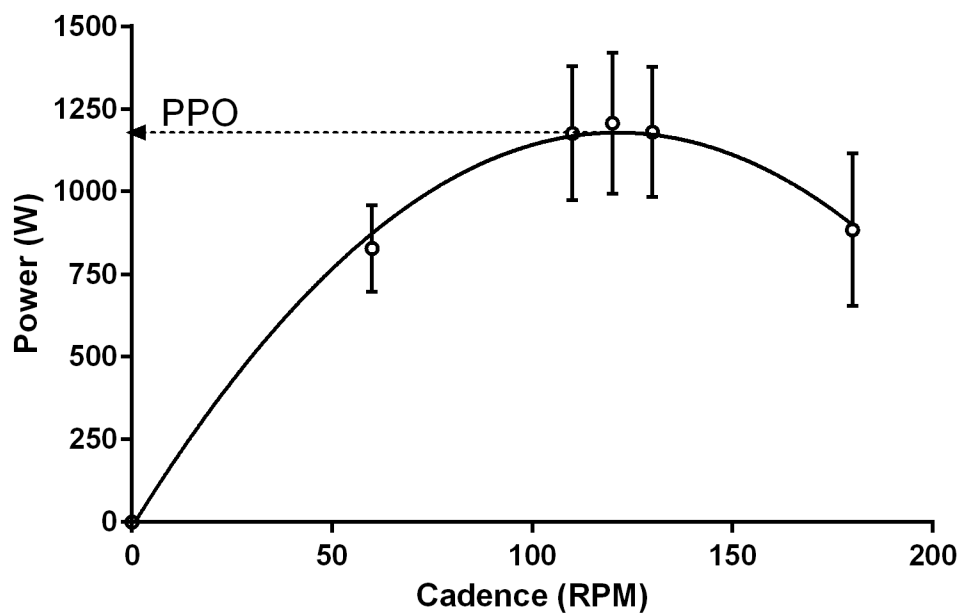
326 Weyand, P.G., Lin, J.E., Bundle, M.W., 2006. Sprint performance-duration relationships are set by
327 the fractional duration of external force application. *Am. J. Physiol. Regul. Integr. Comp.*
328 *Physiol.* 290, R758-765. doi:10.1152/ajpregu.00562.2005

329 Wilson, G.J., Murphy, A.J., 1996. The use of isometric tests of muscular function in athletic
330 assessment. *Sports Med. Auckl. NZ* 22, 19–37.

333 Figure 1.

334 Figure 1: Power-cadence relationship of second order polynomial was formed after performing
335 maximal sprints at 60, 110, 120, 130 and 180 RPM; $R^2 = 0.996$; $y = -0.081x^2 + 19.35x - 13.96$;
336 Mechanical peak power output (PPO) was interpolated and measured at 1108 ± 215 W.

337

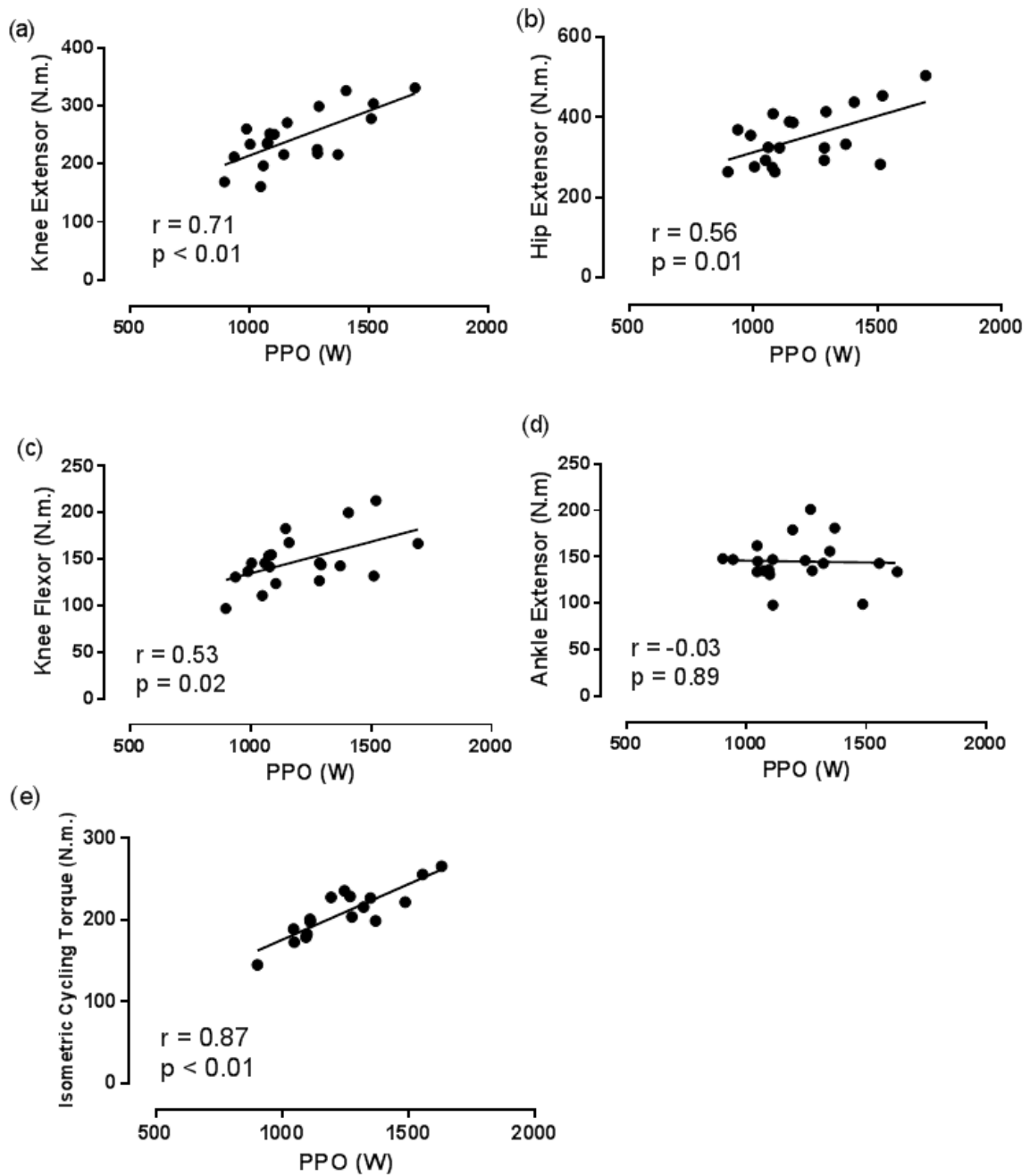


338

339

340 Figure 2

341 Figure 2: Relationship between (a) peak isometric strength of knee extensors and mechanical peak
342 power output (PPO) (b) peak isometric strength of hip extensors and PPO (c) peak isometric strength
343 of knee flexors and PPO (d) peak isometric strength of ankle extensors and PPO (e) peak isometric
344 cycling specific torque and PPO.



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