

Northumbria Research Link

Citation: Parmar, Arran, Keenan, Ashleigh and Barry, Gill (2021) Concurrent validity of the portable gFlight system compared to a force plate to measure jump performance variables. *Physiological Measurement*, 42 (1). 015003. ISSN 0967-3334

Published by: Institute of Physics

URL: <https://doi.org/10.1088/1361-6579/abd236> <<https://doi.org/10.1088/1361-6579/abd236>>

This version was downloaded from Northumbria Research Link:
<https://nrl.northumbria.ac.uk/id/eprint/45148/>

Northumbria University has developed Northumbria Research Link (NRL) to enable users to access the University's research output. Copyright © and moral rights for items on NRL are retained by the individual author(s) and/or other copyright owners. Single copies of full items can be reproduced, displayed or performed, and given to third parties in any format or medium for personal research or study, educational, or not-for-profit purposes without prior permission or charge, provided the authors, title and full bibliographic details are given, as well as a hyperlink and/or URL to the original metadata page. The content must not be changed in any way. Full items must not be sold commercially in any format or medium without formal permission of the copyright holder. The full policy is available online: <http://nrl.northumbria.ac.uk/policies.html>

This document may differ from the final, published version of the research and has been made available online in accordance with publisher policies. To read and/or cite from the published version of the research, please visit the publisher's website (a subscription may be required.)



**Northumbria
University**
NEWCASTLE



UniversityLibrary

ACCEPTED MANUSCRIPT • OPEN ACCESS

Concurrent validity of the portable gFlight system compared to a force plate to measure jump performance variables

To cite this article before publication: Arran Parmar *et al* 2020 *Physiol. Meas.* in press <https://doi.org/10.1088/1361-6579/abd236>

Manuscript version: Accepted Manuscript

Accepted Manuscript is “the version of the article accepted for publication including all changes made as a result of the peer review process, and which may also include the addition to the article by IOP Publishing of a header, an article ID, a cover sheet and/or an ‘Accepted Manuscript’ watermark, but excluding any other editing, typesetting or other changes made by IOP Publishing and/or its licensors”

This Accepted Manuscript is © 2020 Institute of Physics and Engineering in Medicine.

As the Version of Record of this article is going to be / has been published on a gold open access basis under a CC BY 3.0 licence, this Accepted Manuscript is available for reuse under a CC BY 3.0 licence immediately.

Everyone is permitted to use all or part of the original content in this article, provided that they adhere to all the terms of the licence <https://creativecommons.org/licenses/by/3.0>

Although reasonable endeavours have been taken to obtain all necessary permissions from third parties to include their copyrighted content within this article, their full citation and copyright line may not be present in this Accepted Manuscript version. Before using any content from this article, please refer to the Version of Record on IOPscience once published for full citation and copyright details, as permissions may be required. All third party content is fully copyright protected and is not published on a gold open access basis under a CC BY licence, unless that is specifically stated in the figure caption in the Version of Record.

View the [article online](#) for updates and enhancements.

Title

Concurrent validity of the portable gFlight system compared to a force plate to measure jump performance variables

Authors

Arran Parmar MRes¹, Ashleigh Keenan BSc¹, Gill Barry PhD¹

1. Department of Sport, Exercise and Rehabilitation

Faculty of Health and Life Sciences

Northumbria University

Newcastle-Upon-Tyne

NE1 8ST

United Kingdom

Corresponding Author

Arran Parmar

Department of Sport, Exercise and Rehabilitation

Faculty of Health and Life Sciences

Northumbria University

Newcastle-Upon-Tyne, NE1 8ST

United Kingdom

Email: arran.parmar@northumbria.ac.uk

Accepted Manuscript

Abstract

Objective: Lower-limb strength and power is commonly assessed indirectly by measuring jump performance. A novel portable system (gFlight) that can be used in applied settings provides measures of jump performance. The aim of this study was to validate jump performance measures provided by the gFlight to those provided by a force plate.

Approach: Thirty-six participants performed three countermovement jump and drop jump trials. Jump height, contact time, and reactive strength index were simultaneously recorded by a force plate and gFlight sensors to assess concurrent validity.

Main Results: The gFlight provided significantly higher measures of jump height during the countermovement jump (Mean: $+8.79 \pm 4.16$ cm, 95% CI: $+7.68$ to 9.90 cm, $P < 0.001$) and drop jump (Mean: $+4.68 \pm 3.57$ cm, 95% CI: $+3.73$ to 5.63 cm, $P < 0.001$) compared to the force plate. The gFlight sensors displayed significantly higher measures of reactive strength index (Mean: $+0.48 \pm 0.39$ m·s⁻¹, 95% CI: $+0.37$ to 0.58 m·s⁻¹, $P < 0.001$) and lower measures of contact time (Mean: -0.036 ± 0.028 s, 95% CI: -0.044 to -0.029 s, $P < 0.001$) during the drop jump compared to the force plate. The bias displayed by the gFlight for jump height, contact time and reactive strength index measures are reduced using corrective equations.

Significance: The gFlight sensors are a cost-effective, portable measurement system with high concurrent and ecological validity for the objective measurement of jump performance in applied settings. Corrective equations should be used to reduce measurement biases so comparisons can be made to force plate measurements of jump performance.

Keywords: Countermovement jump, drop jump, jump measurement, field-based, applied practitioners.

List of abbreviations:

JH, jump height; CMJ, countermovement jump; DJ, drop jump; SSC, stretch-shortening cycle; RSI, reactive strength index; SD, standard deviation; CV, coefficient of variation; SEE, standard error of estimate; CI, confidence interval.

Introduction

Lower-limb power is commonly assessed indirectly by measuring jump height (JH) performance during vertical jumping tasks such as the countermovement jump (CMJ) and drop jump (DJ) (1–3). The measurement of JH is a frequently used method to assess and monitor physical performance and adaptations by coaches and researchers (4,5), along with being one of the most prevalent activities performed in a wide range of sports (6). Assessing lower-limb performance during jumping tasks provides coaches and researchers with information relating to the utilisation of the stretch shortening cycle (SSC) and reactive strength index (RSI) during the CMJ and DJ, respectively (5,7).

Force plates are considered the ‘gold standard’ to measure jump performance (8,9). Force plates are mechanical systems that provide measurements of ground reaction forces and moments involved with human movement (10), however, these are often expensive (~20k£), bulky and require specialist software to collect and analyse data. The use of force plates to measure JH where access to laboratory facilities are limited are therefore impractical, however, applied practitioners still need to assess and monitor the physical performance and readiness of the athletes they support.

In order to make traditional lab-based performance tests more accessible, advances in technology have provided applied practitioners and athletes with access to field-based measures of JH that can be used in their own environments. These include contact mats (Just Jump system), velocity systems (GymAware), linear position transducers (MyoTest, Vertec), optical photoelectric cells (OptoJump), and mobile phone applications (MyJump), (6,9,11,12). These field-based alternatives, however, all use different software and calculations to provide JH measurements meaning results can vary depending on the system used. With portable and wearable technologies increasing in popularity, more research is being published to evaluate the reliability and validity of these measurement systems (13,14).

Recently in 2018, a novel portable measurement system was developed (Exsurgo gFlight v2,) that can fit into a small bag and connects to a free downloadable smartphone application (gTechAMS, Exsurgo Technologies, LLC) via Bluetooth. The system consists of two photoelectric boxes; one transmitter and one receiver that are placed at a maximum of 5.8 m apart at floor level. The gFlight measures JH via time in air, CT and RSI, with participants instructed to stand with their fifth metatarsal in line with the beam. The portability and relatively low price (\$399) of the gFlight makes this system an accessible option for applied practitioners, as well as improving the ecological validity of the measurements taken. The validity of the gFlight however is unknown, with no studies currently published evaluating the validity of the measures provided by the gFlight system against those provided by the ‘gold standard’ force plate.

1
2
3 The aim of this study is to provide a novel evaluation of the concurrent validity of the gFlight
4 compared to the 'gold standard' force plate to measure JH, CT, and RSI during a countermovement
5 jump and drop jump. The evaluation of this novel measurement system will provide researchers and
6 practitioners with knowledge as to the validity of the measures provided by the gFlight for the first
7 time.
8
9
10

11 12 13 **Method**

14 **Participants**

15 With institutional ethics approved by Northumbria University research and ethics committee, 36 young
16 healthy adults (27 male, 9 female) participated. The age, stature and mass of participants, reported as
17 Mean \pm SD, were 22.0 ± 4.4 yrs; height: 1.75 ± 0.08 m; 74.87 ± 11.88 kg. The inclusion criteria for
18 participation in this study were that participants had to be aged 18-35 years, and free from physical
19 limitations or musculoskeletal injuries that could affect their ability to perform the testing procedures.
20 Participants were excluded if they had an injury to the lower limb or had any condition that would affect
21 jumping performance. Participants represented a wide range of abilities and training status from
22 recreational to highly trained, participating in 1.5 to 14 h of moderate to strenuous physical activity per
23 week, as defined in the American College of Sports Medicine (ACSM) Physical Activity Guidelines
24 (15). This was to ensure the gFlight system could be validated across a wide range of jump heights. All
25 participants were asked to refrain from strenuous exercise in the 24 h prior to testing. Testing procedures
26 were conducted on two separate occasions separated by 1-week at the same time of day (1300-1700),
27 with participants wearing the same pair of their own athletic shoes with cushioning for all trials.
28
29
30
31
32
33
34
35
36
37

38 **Study Design**

39 All participants performed 3 maximal trials of the countermovement jump (CMJ) and the drop jump
40 (DJ) with hands placed on the hips throughout, following a standardized 10 min warm-up. Data for each
41 trial were simultaneously recorded using a floor integrated force plate (AMTI Biovac 1100, Watertown,
42 MA, USA) (criterion instrument) and a pair of Exsurgo gFlight sensors (Exsurgo, Virginia, USA)
43 (practical instrument) to assess the concurrent validity of this latter system, with the averages of the 3
44 CMJ and DJ trials used for further analysis. The dependent variables were jump heights of the CMJ and
45 DJ, and the contact time and reactive strength index (RSI) of the DJ. The independent variables were
46 the measurement tools; specifically, the force plate as the gold-standard criterion measure, and the
47 gFlight sensors as the practical experimental measure.
48
49
50
51
52
53
54

55 **Procedures**

56 Upon arrival to the laboratory, a full explanation of the experimental protocol and procedures was
57 provided to participants. Following this, participants completed a standardized 10 min warm-up led by
58 the principal investigator following the raise, activate, mobilise and potentiate (RAMP) protocol (16)
59
60

1
2
3 consisting of movements similar to those detailed in similar previous studies (6,17,18). At the end of
4 the warm-up participants performed 3 submaximal CMJ and 3 submaximal DJ at 50, 75, and 90%
5 perceived maximum effort, familiarizing participants with the jump protocols. Each participant
6 subsequently performed the 3 maximal CMJ trials and the 3 maximal DJ trials on the force plate and
7 between the gFlight sensors. All jump trials were separated by 30 s of rest, with 2 min between the
8 types of jumps.
9
10
11
12
13

14 For the standardisation of all jumps, participants kept their hands on their hips throughout the entire
15 movement and were instructed to jump vertically with as little horizontal displacement as possible and
16 land in the same place as take-off. For the CMJ, participants stood in an upright position with feet
17 approximately shoulder width apart. From this position, participants were instructed to squat to
18 approximately 90° of knee flexion as fast as possible before then jumping as high as possible. For the
19 DJ, participants stood in an upright position with feet shoulder width apart on a 0.30 m box before
20 stepping forwards off of the box. Upon contact with the ground, participants jumped as high as possible,
21 as quickly as possible, attempting to achieve the greatest jump height with the least ground contact time
22 (19). Jump trials not meeting these procedures were deemed invalid and participants repeated the trial.
23
24
25
26
27
28
29

30 The Exsurgo gFlight sensors were placed at the extremities of the force platform without touching it, in
31 a parallel and horizontal position to one another at a distance of 0.56 m (Figure 1). The Exsurgo gFlight
32 sensors were connected via Bluetooth to an iPhone SE (Apple Inc., USA) to record jump trials on the
33 Exsurgo gtech application, with all dependent variables (jump height, contact time, and RSI)
34 automatically calculated. The force plate (AMTI Biovac 1100, Watertown, MA, USA) was integrated
35 into the floor to measure the vertical ground reaction force (VGRF) during jumping at a sampling rate
36 of 2000 Hz (Figure 1). The force time trace recorded for each trial was used to directly calculate all
37 dependent variables (jump height, contact time, and RSI). Contact times and flight times were obtained
38 using a threshold of >10 N to determine contact and <10 N to determine flight (20). Jump height from
39 force plate data was estimated as $9.81 \times \text{flight time}^2/8$ (1). The RSI was calculated by dividing the jump
40 height by the contact time (7,21).
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

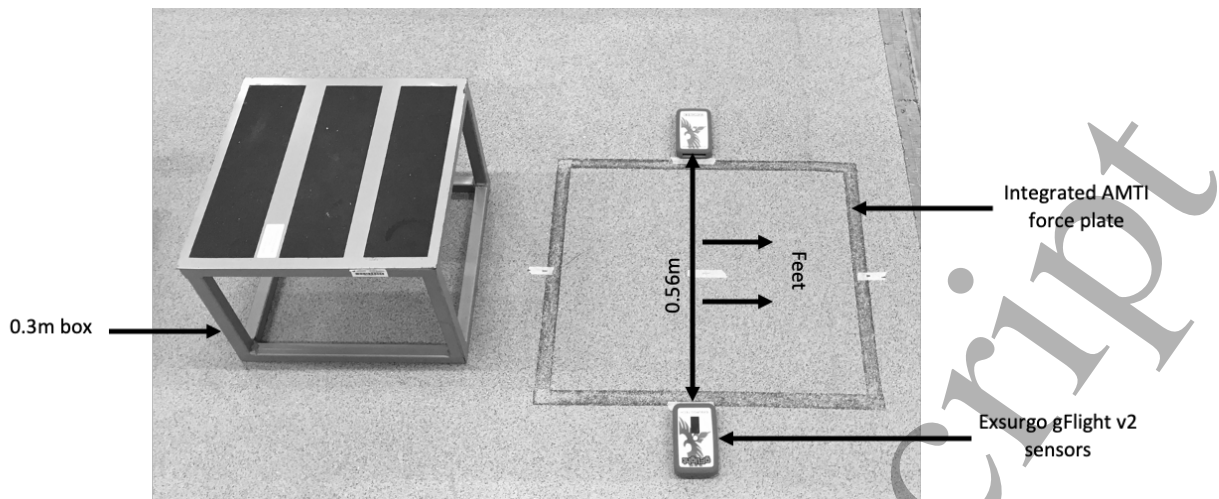


Figure 1 - Experimental setup showing the 2 measuring tools, distance between the gFlight sensors, the 0.3m box for drop jumps, and the position of the feet on the force plate recording area.

Statistical Analyses

All data are presented as mean \pm standard deviation (SD). Normality was assessed by visual inspection of box plots for all dependent variables before analyses. The dependent variables obtained from the 3 CMJ trials and the 3 DJ trials performed by each participant were averaged for further analyses. Paired samples t-tests (and associated 95% confidence intervals) were used to detect systematic differences (also referred to as bias) between tools (validity) for all dependent variables. Concurrent validity between measurement tools for all dependent variables were examined using bivariate linear regression, coefficient of variation (CV), and Pearson's correlation coefficient (r). The Standard Error of Estimate (SEE) was calculated to assess the accuracy of the predictive equation from the linear regression. The coefficient of determination (R^2) was calculated to demonstrate the relationship between the dependent variables measured from the two measurement tools. Effect sizes (d) were calculated to determine the magnitude of differences between the two measurement tools for all dependent variables. A modified scale was used for the interpretation of d ; $d < 0.2$ as trivial, 0.2-0.6 as small, 0.6-1.2 as moderate, 1.2-2.0 as large, 2.0-4.0 as very large, and > 4.0 as extremely large (22). The magnitude of correlation (r) was interpreted as; < 0.10 as trivial, 0.10-0.30 as small, 0.30-0.50 as moderate, 0.50-0.70 as large, 0.70-0.90 as very large, and 0.90-1.00 as almost perfect (23). All analyses were performed using the Microsoft Excel (2013) statistical package using a spreadsheet for validity (24). Statistical significance was accepted when $P < 0.05$.

Results

Jump Height

The gFlight sensors demonstrated a *very large* agreement with the force plate for the measurement of jump height (JH) in both the CMJ ($r = 0.83$) and the DJ ($r = 0.83$). Despite this agreement, the gFlight displayed a significant systematic bias with higher measures of JH provided in comparison to the force

1
2
3 plate during the CMJ (Mean: $+8.79 \pm 4.16$ cm, 95% CI: $+7.68$ to 9.90 cm, d : 1.25, $P < 0.001$) and the DJ
4 (Mean: $+4.68 \pm 3.57$ cm, 95% CI: $+3.73$ to 5.63 cm, d : 0.83, $P < 0.001$) (Table 1). The systematic bias
5 demonstrated between the two measurement tools increased with increasing JH, as predicted by the
6 linear regression equations for both the CMJ (Figure 2A) and the DJ (Figure 3A); with 69% and 68%
7 of the variance in JH explained by the respective equations. The standard error of estimate (SEE) was
8 ± 3.80 cm during the CMJ and ± 2.81 cm during the DJ. The coefficient of variation (CV) describing the
9 concurrent validity between measurement tools were 13.60% for the CMJ and 13.40% for the DJ (Table
10 1).
11
12
13
14
15
16

17 Correcting the gFlight measurement of JH using the linear regression equations for the CMJ: corrected
18 CMJ height = $0.7595 \times \text{raw gFlight JH} + 0.6306$; and the DJ: corrected DJ height = $0.647 \times \text{raw gFlight}$
19 $\text{JH} + 4.7173$; reduced the significant systematic bias displayed between the two measurement tools in
20 both the CMJ (Mean: 0.00 ± 3.77 cm, 95% CI: -1.00 to 1.01 cm, $d < 0.001$, $P = 0.99$) and the DJ (Mean:
21 0.00 ± 2.78 cm, 95% CI: -0.74 to 0.74 cm, $d < 0.001$, $P = 0.99$) (Table 2). The corrected gFlight JH
22 measures demonstrated *very large* agreement with the force plate in both the CMJ ($r = 0.83$) and the DJ
23 ($r = 0.83$), with the linear regression equations displaying a *nearly perfect* relationship in the CMJ ($y =$
24 $1x + 6 \times 10^{-6}$; Figure 2B) and the DJ ($y = 1x - 0.0001$, Figure 3B).
25
26
27
28
29
30
31

32 **Contact time and Reactive Strength Index**

33 The gFlight sensors displayed a significant systematic bias for the measurement of contact time and
34 reactive strength index (RSI), with a lower measure of contact time (Mean: -0.036 ± 0.028 s, 95% CI:
35 -0.044 to -0.029 s, d : -0.75 , $P < 0.001$) and a higher measure of RSI (Mean: $+0.48 \pm 0.39$ m·s⁻¹, 95% CI:
36 $+0.37$ to 0.58 m·s⁻¹, d : 0.97, $P < 0.001$) provided compared to the force plate (Table 1). Pearson
37 correlation values demonstrated *very large* agreement between measurement tools for both contact time
38 ($r = 0.83$) and RSI ($r = 0.75$). The systematic bias displayed by the gFlight sensors compared to the
39 force plate for the measurement of contact time was consistent as predicted by the linear regression
40 equation, with a SEE of ± 0.028 s and the equation explaining 69% of the variance observed (Figure
41 4A). The systematic bias observed between the two measurement tools increased with increasing RSI
42 as predicted by the linear regression equation, with a SEE of ± 0.25 m·s⁻¹ and the equation explaining
43 56% of the variance observed (Figure 5A). The CV values describing the concurrent validity between
44 measurement tools for contact time and RSI were 13.70% and 26.20%, respectively (Table 1).
45
46
47
48
49
50
51
52
53

54 Correcting the gFlight measures of contact time and RSI using the linear regression equations: corrected
55 DJ contact time = $0.9497 \times \text{raw gFlight contact time} + 0.0458$; and corrected DJ RSI = $0.4781 \times \text{raw}$
56 $\text{gFlight RSI} + 0.2994$; reduced the significant systematic bias displayed between the two measurement
57 tools for contact time (Mean: 0.00 ± 0.028 s, 95% CI: -0.008 to 0.008 s, $d < 0.001$, $P = 0.99$) and RSI
58 (Mean: 0.00 ± 0.25 m·s⁻¹, 95% CI: -0.07 to 0.07 m·s⁻¹, $d < 0.001$, $P = 0.99$) (Table 2). The corrected
59
60

1
2
3 gFlight measures of contact time ($r = 0.83$) and RSI ($r = 0.75$) demonstrated *very large* agreement with
4 the force plate, with the linear regression equations displaying a *nearly perfect* relationship for contact
5 time ($y = 1x + 8 \times 10^{-7}$; Figure 4B) and RSI ($y = 0.9999x + 1 \times 10^{-5}$; Figure 5B).
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60

Accepted Manuscript

Table 1 – Concurrent validity between the gFlight and force plate for the measurement of all dependent variables during the Countermovement Jump (CMJ) and the Drop Jump (DJ). Data presented as Mean \pm Standard Deviation.

Jump	Variable	gFlight (95% CI)	Force plate (95% CI)	Systematic Bias (95% CI)	CV%	Effect size (<i>d</i>)	Inference
CMJ	Height (cm)	39.16 \pm 7.34 (37.20 to 41.12)	30.37 \pm 6.73 (28.58 to 32.16)	+8.79 \pm 4.16* (7.68 to 9.90)	13.60%	1.25	Large
	Height (cm)	26.62 \pm 6.31 (24.93 to 28.30)	21.94 \pm 4.94 (20.62 to 23.26)	+4.68 \pm 3.57* (3.73 to 5.63)	13.40%	0.83	Moderate
DJ	Contact Time (s)	0.194 \pm 0.045 (0.182 to 0.206)	0.230 \pm 0.051 (0.217 to 0.244)	-0.036 \pm 0.028* (-0.044 to -0.029)	13.70%	-0.75	Moderate
	RSI (m·s⁻¹)	1.49 \pm 0.58 (1.33 to 1.64)	1.01 \pm 0.37 (0.91 to 1.11)	+0.48 \pm 0.39* (0.37 to 0.58)	26.20%	0.97	Moderate

CMJ; Countermovement Jump, DJ; Drop Jump, 95% CI; 95% Confidence Interval, CV; Coefficient of Variation, RSI; Reactive Strength Index

*Significant bias displayed by the gFlight measure compared to the force plate measure ($P < 0.001$).

Table 2 - Concurrent validity between the force plate and the corrected gFlight measures using the respective linear regression equations for all dependent variables during the Countermovement Jump (CMJ) and the Drop Jump (DJ). Data presented as Mean \pm Standard Deviation.

Jump	Variable	Corrected gFlight (95% CI)	Force plate (95% CI)	Systematic Bias (95% CI)	CV%	Effect size (<i>d</i>)	Inference
CMJ	Height (cm)	30.37 \pm 5.57 (28.88 to 31.86)	30.37 \pm 6.73 (28.58 to 32.16)	0.00 \pm 3.77 (-1.00 to 1.01)	13.60%	<0.001	Trivial
	Height (cm)	21.94 \pm 4.09 (20.85 to 23.03)	21.94 \pm 4.94 (20.62 to 23.26)	0.00 \pm 2.78 (-0.74 to 0.74)	13.50%	<0.001	Trivial
DJ	Contact Time (s)	0.230 \pm 0.042 (0.219 to 0.242)	0.230 \pm 0.051 (0.217 to 0.244)	0.00 \pm 0.028 (-0.008 to 0.008)	13.50%	<0.001	Trivial
	RSI (m·s⁻¹)	1.01 \pm 0.28 (0.94 to 1.09)	1.01 \pm 0.37 (0.91 to 1.11)	0.00 \pm 0.25 (-0.07 to 0.07)	26.20%	<0.001	Trivial

CMJ; Countermovement Jump, DJ; Drop Jump, 95% CI; 95% Confidence Interval, CV; Coefficient of Variation, RSI; Reactive Strength Index

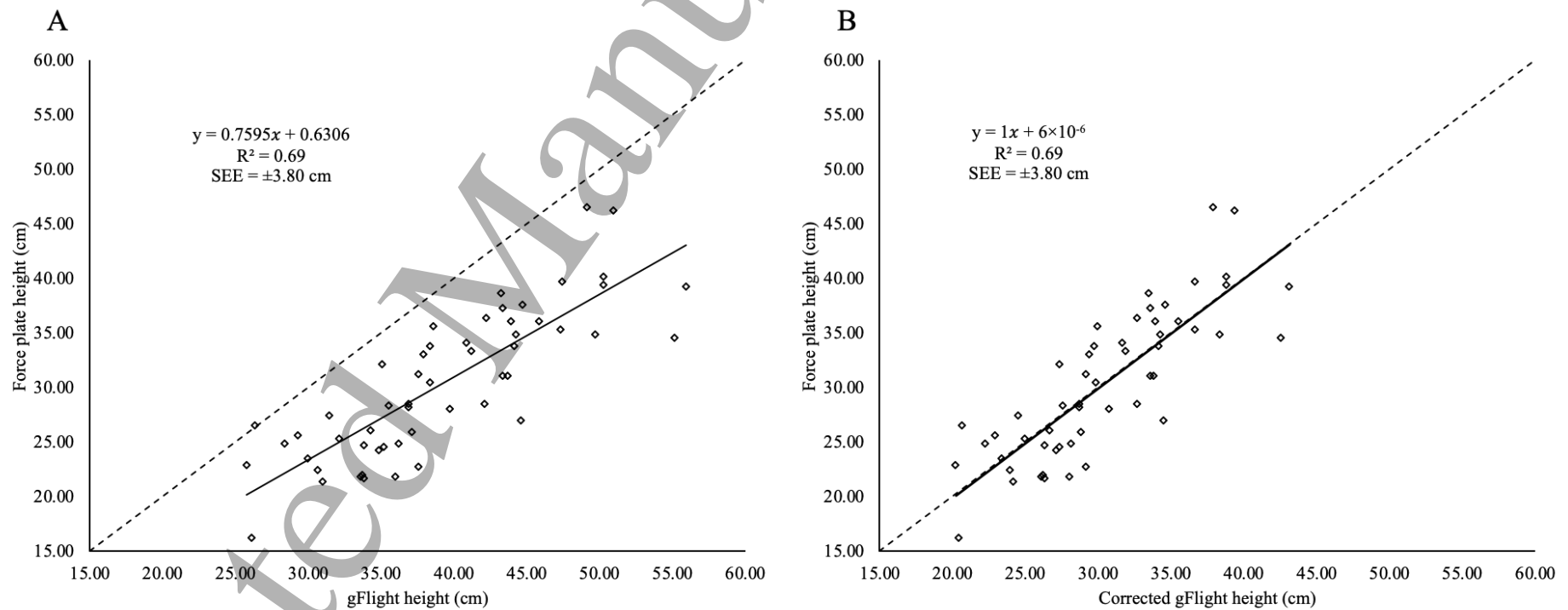


Figure 2 – Panel A: Correlation between the measurement of jump height from the force plate and gFlight sensors during the countermovement jump. The dotted line represents the line of identity (force plate height = gFlight height). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE). **Panel B:** Correlation between the measurement of jump height from the force plate and gFlight sensors after correcting trials using the regression equation (corrected countermovement jump height = $0.7595 \times$ raw gFlight jump height + 0.6306), during the countermovement jump. The dotted line represents the line of identity (force plate height = corrected gFlight height). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE).

Data points represent the average jump height values taken from the three trials performed by each participant.

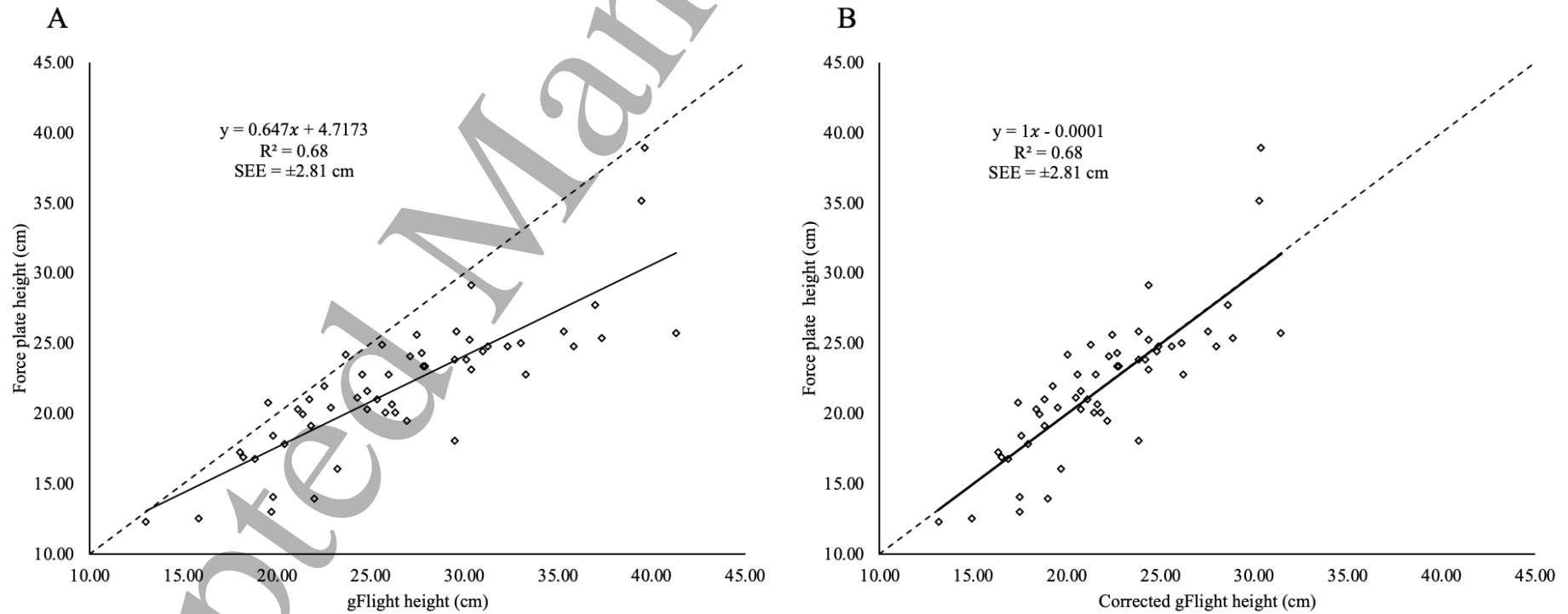


Figure 3 – Panel A: Correlation between the measurement of jump height from the force plate and gFlight sensors during the drop jump. The dotted line represents the line of identity (force plate height = gFlight height). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE). **Panel B:** Correlation between the measurement of jump height from the force plate and gFlight sensors after correcting trials using the regression equation (corrected drop jump height = $0.647 \times$ raw gFlight jump height + 4.7173), during the drop jump. The dotted line represents the line of identity (force plate height = corrected gFlight height). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE). Data points represent the average jump height values taken from the three trials performed by each participant.

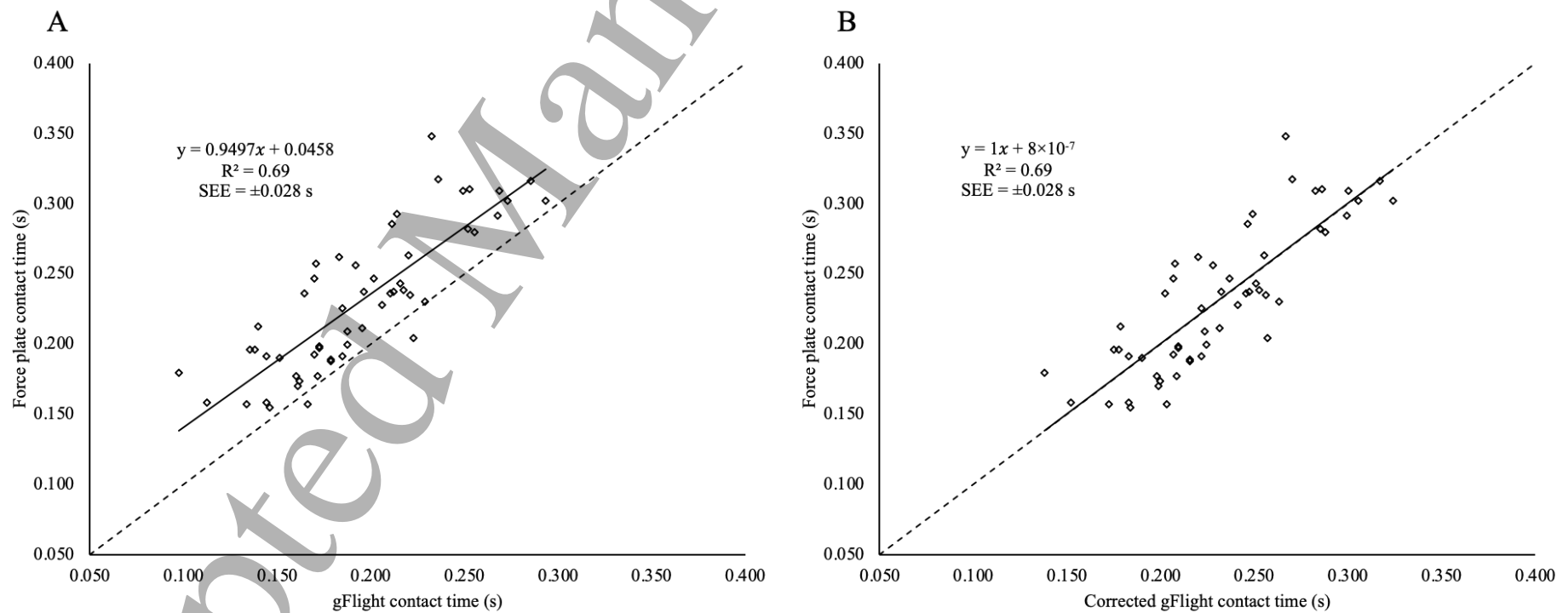


Figure 4 – Panel A: Correlation between the measurement of contact time from the force plate and gFlight sensors during the drop jump. The dotted line represents the line of identity (force plate contact time = gFlight contact time). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE). **Panel B:** Correlation between the measurement of contact time from the force plate and gFlight sensors after correcting trials using the regression equation (corrected drop jump contact time = $0.9497 \times$ raw gFlight contact time + 0.0458), during the drop jump. The dotted line represents the line of identity (force plate contact time = corrected gFlight contact time). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE).

Data points represent the average contact time values taken from the three trials performed by each participant.

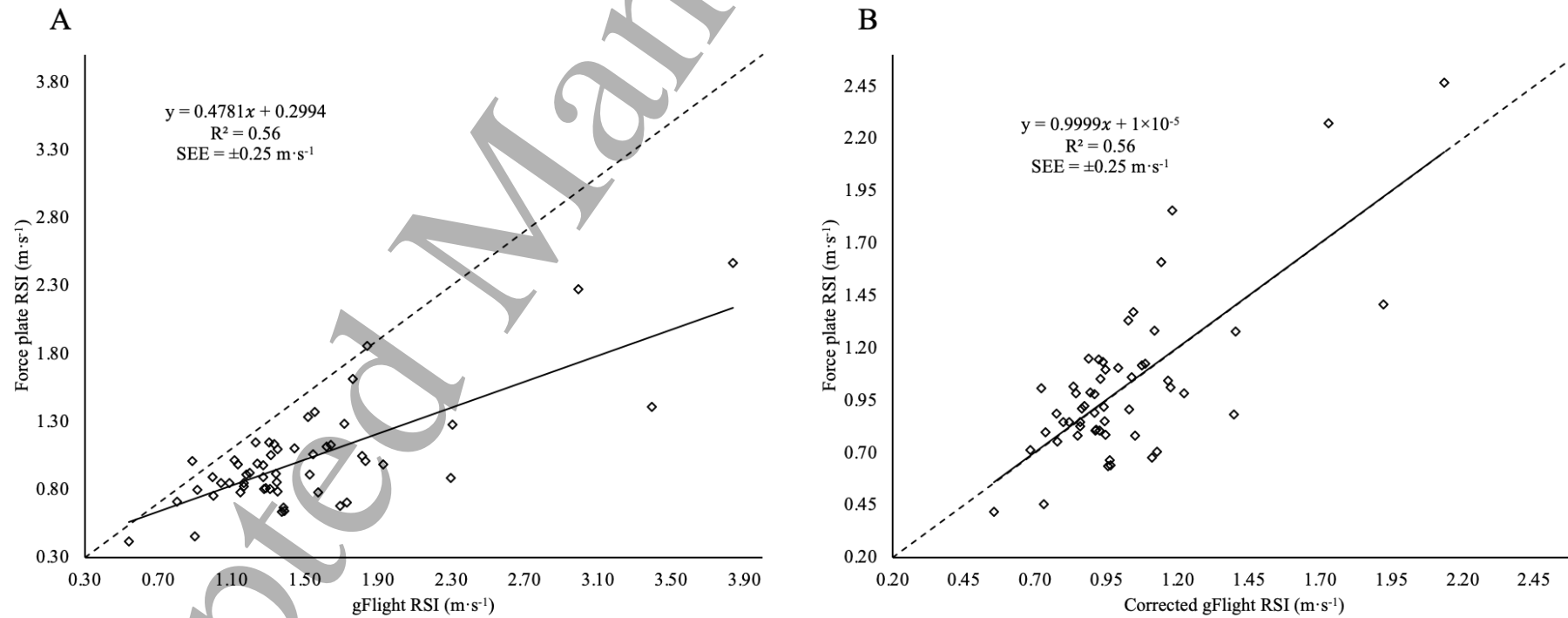


Figure 5 – Panel A: Correlation between the measurement of reactive strength index (RSI) from the force plate and gFlight sensors during the drop jump. The dotted line represents the line of identity (force plate RSI = gFlight RSI). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE). **Panel B:** Correlation between the measurement of RSI from the force plate and gFlight sensors after correcting trials using the regression equation (corrected drop jump RSI = $0.4781 \times$ raw gFlight RSI + 0.2994), during the drop jump. The dotted line represents the line of identity (force plate RSI = corrected gFlight RSI). The solid line shows the linear regression fit of the two measurement tools with the associated regression equation, coefficient of determination (R^2), and standard error of estimate (SEE).

Data points represent the average RSI values taken from the three trials performed by each participant.

Discussion

The aim of this study was to evaluate the concurrent validity of the gFlight sensors in comparison to a force plate to measure JH, CT and RSI during a countermovement jump and drop jump. This is the first study to evaluate the novel gFlight system to a 'gold standard' criterion force plate, providing practical information pertaining to the validity of the gFlight sensors for use in applied settings. The major findings from this study were that the gFlight system demonstrated strong concurrent validity compared to the force plate for all measures during the CMJ and DJ. Despite this, a significant systematic bias was displayed between the two measurement tools, as the gFlight provided higher measures of JH and RSI during the countermovement jump and drop jump, respectively, with the observed bias increasing with increasing JH and RSI. Similarly, measurements of CT provided by the gFlight were systematically lower than those provided by the force plate, however the bias observed was consistent irrespective of the contact time measurement. Nevertheless, the gFlight demonstrated *very large* agreement for all measures (r values ranging between 0.75 to 0.83) between the gFlight and force plate. The use of corrective equations derived from the linear regression equations reduced the systematic bias observed between measurement tools for all measures, thereby making this a potentially valid measurement tool to use within applied settings.

The higher systematic bias observed between the gFlight and force plate for the measurement of jump height contrasts previous research evaluating the validity of similar systems using photoelectric cells (Optojump) to estimate JH, from the measurement of flight time. Differences between measures of jump height using the Optojump are consistently reported to be systematically lower than force plate measures of JH, typically attributed to the photoelectric cells being raised off of the ground leading to lower measures of flight time and in turn JH (6,18,25). The measurement of flight time from photoelectric cell devices is dependent upon the detection of take-off and landing (6,25). The detection area of the gFlight system is relatively small in comparison to the Optojump, therefore any horizontal displacement exhibited during the flight phase of a jump might affect the measurement of flight time due to the landing location being different to the take-off location (18). The smaller detection area of the gFlight might therefore overestimate flight time due to differences in the detection of take-off and landing, and in turn the JH measure. In comparison, the Optojump system has a larger detection area, therefore any horizontal displacement exhibited during the flight phase of a jump will not affect the JH measure provided. This difference in the size of the detection area perhaps explains the contrasting biases observed compared to the force plate for the measurement of JH. Another field-based alternative to measure JH via flight time is a smartphone application, that reportedly provides a measure of JH similar to that provided by a force plate (mean bias = 0.9 ± 0.2 cm) (17). Although the reported bias is lower than that shown here for the gFlight, the smartphone application relies on the user filming the jump trial at a suitable frame rate along with correctly identifying the take-off and landing frames for

1
2
3 the calculation of flight time and hence JH (17). The additional input required when using the
4 smartphone application in comparison to the gFlight might reduce the systematic bias observed,
5 however the gFlight offers a method to measure JH instantly without additional input, along with the
6 presented corrective equations reducing the bias. Similarly, another alternative to force plates is the use
7 of an accelerometer to measure JH via flight time, with the reported mean bias (3.6 ± 0.1 cm) also less
8 than the gFlight (25). The use of the accelerometer however requires specific and consistent placement
9 on the participant for reliable JH measurements, along with specialist software to analyse the data.
10 Furthermore, despite the accelerometer being a more cost-effective option than force plates, the price
11 is still relatively higher than the gFlight system (26). When compared to other field-based alternatives
12 for the measurement of JH, the gFlight demonstrates a higher systematic bias for the measurement of
13 JH during both CMJ and DJ modalities (8,17,25,26). Nevertheless, the portability, low cost and
14 accessibility might appeal to applied practitioners and researchers despite the greater systematic bias
15 demonstrated compared to other field-based alternatives. With this in mind, the use of corrective
16 equations presented herein can improve the validity of the gFlight system. The present findings show
17 the corrective equations for CMJ JH (corrected CMJ height = $0.7595 \times$ raw gFlight JH + 0.6306) and
18 DJ JH (corrected DJ height = $0.647 \times$ raw gFlight JH + 4.7173) lead to the *large* (CMJ JH: $+8.79 \pm$
19 4.16 cm, $d = 1.25$) and *moderate* (DJ JH: $+4.68 \pm 3.57$ cm, $d = 0.83$) systematic biases to be reduced to
20 *trivial* (CMJ JH: 0.00 ± 3.77 , $d = <0.001$; DJ JH: 0.00 ± 2.78 cm, $d = <0.001$) biases, effectively
21 reducing the difference demonstrated between the force plate and gFlight. The gFlight sensors can
22 therefore be considered valid measures of JH in both the CMJ and DJ with the use of the proposed
23 corrective equations, which have been derived from a population of varied athletic ability.

24
25
26
27
28
29
30
31
32
33
34
35
36
37
38 The current study sought to evaluate measures of contact time and reactive strength index (RSI)
39 provided by the gFlight during a DJ, as this information is relevant to practitioners attempting to assess
40 the reactive stretch shortening cycle abilities (SSC) of the athletes they support (1,5,7). The RSI
41 provides a measure of an athletes' ability to develop maximal force in minimal time through the
42 utilisation of the fast SSC, derived from the measurement of jump height divided by the ground contact
43 time (7). The SSC consists of an eccentric muscle contraction immediately followed by a concentric
44 muscle contraction, with a shorter time between these phases facilitating a greater ability to generate
45 force due the ability to utilise the SSC (1,7). The gFlight sensors provided systematically lower and
46 higher measures of CT and RSI, respectively compared to the force plate. As RSI is calculated from
47 jump height and contact time (7,20), the higher JH and lower CT measures provided by the gFlight
48 result in the higher reactive strength index demonstrated in comparison to the force plate. The validity
49 of CT and RSI measures from field-based measurement tools during a DJ is limited, as previous
50 research has focussed primarily on vertical jumping tasks such as the CMJ or squat jump (3,6,11,13,17).
51 The few studies that have evaluated measures of CT and RSI provided by field-based devices have
52 reported varied findings; with lower measures of CT provided by the *MyJump 2* application (27) and
53
54
55
56
57
58
59
60

1
2
3 the MyoTest accelerometer (28), and higher measures of CT provided by the Optojump (20,29) in
4 comparison to force plate measures. Similarly, measures of RSI have been reported to be lower for the
5 Optojump (20), similar for the MyoTest accelerometer (28), and higher for the *MyJump 2* application
6 in comparison to force plate measures. The different measures of contact time and RSI provided by
7 these various measurement tools are most likely attributed to the different methods of detection along
8 with the study design. Such differences include the use of photoelectric systems, video recordings,
9 linear position transducers, and accelerometers all of which use various methods to determine CT and
10 RSI. Furthermore, measures of CT and RSI have been from hopping tasks rather than a drop jump (28),
11 and various drop heights implemented for the DJ task (20,27,29). The differences in contact time and
12 RSI measures provided by the gFlight system in comparison to the force plate are not dissimilar from
13 the differences demonstrated by the aforementioned field-based alternatives. When compared to the
14 reported differences in CT and RSI demonstrated by the Optojump (due to this system also utilising
15 photoelectric cells), the gFlight does provide higher RSI measures and lower CT measures. This is most
16 likely due to the size of the detection area, as previously explained. Nevertheless, in comparison to other
17 field-based alternatives, the gFlight sensors offer a portable, time efficient and cost-effective option for
18 applied practitioners and researchers alike to obtain objective measures of DJ performance. To allow
19 comparisons of contact time and RSI measures to be made between the gFlight and force plate, the
20 corrective equations presented in this study (corrected DJ contact time = $0.9497 \times \text{raw gFlight contact time} + 0.0458$;
21 corrected DJ RSI = $0.4781 \times \text{raw gFlight RSI} + 0.2994$) can be used to reduce the
22 systematic bias observed between the measurement tools. These equations can therefore be used to
23 provide valid measures of CT and RSI in applied settings that have been derived from the gFlight
24 sensors.

39 **Limitations**

40
41
42 The measurements of jump height, contact time, and reactive strength index provided by the gFlight in
43 this study can be considered acceptable and valid when compared to the differences demonstrated by
44 other validated field-based alternatives. The evaluation of the gFlight sensors, however, does not come
45 without its limitations. The high coefficient of variation (CV) values reported (13.50 – 26.20%) are
46 considered to be unacceptable according to previous studies reporting CV values <10% to be acceptable
47 for biomechanical variables (30,31). The high variability observed in this study is most likely attributed
48 to the mixed athletic ability of the participants, as demonstrated by the large range of scores for jump
49 height (CMJ: 25.76 to 55.94 cm; DJ: 12.96 to 41.27 cm), contact time (0.097 to 0.293), and reactive
50 strength index (0.54 to $3.84 \text{ m}\cdot\text{s}^{-1}$) measured by the gFlight sensors. It is also acknowledged that
51 horizontal displacement can vary between participants when performing jumps, which combined with
52 the small detection area of the gFlight sensors could potentially contribute further to the observed
53 measurement variability, however this was not measured. Furthermore, this variability might have been
54
55
56
57
58
59
60

present during participants perceived maximum effort warm-up trials, however, these jumps were not measured which is a possible limitation. Whilst we acknowledge the CV values can be considered unacceptable, the mixed athletic ability of the sample population allows the concurrent validity of the gFlight sensors to be tested across a wide range of jump heights. A further limitation lies in the familiarity of the participants to perform the jump protocols. Despite familiarisation and instruction, there might still be inherent learning effects, especially for the performance of the DJ protocol for participants that do not perform such activities regularly, therefore contributing to the large variation observed. In addition, it is worth mentioning the number of trials where incomplete data was provided by the gFlight when participants performed their jumps. Of the 324 trials performed, the gFlight provided incomplete data on 6 occasions (1.85%), however, this low rate had no significant impact upon the ability to complete the tests and the subsequent data analyses. It is suggested future research examining the validity of the gFlight sensors should focus on populations in which jumping activities are performed regularly, such as basketball, volleyball and netball. Such research would therefore be able to evaluate if the systematic bias and variation observed in a mixed population is evident in trained athletic populations, along with if the corrective equations presented herein are applicable to these populations.

Conclusion

This study evaluated the concurrent validity of the novel gFlight sensors to provide measures of jump height, contact time, and reactive strength index during a CMJ and DJ in comparison to those provided by a 'gold standard' force plate. The gFlight sensors provided valid measures of the dependent variables in both jump modalities, however systematic biases were demonstrated. The use of corrective equations should be used to reduce these biases and allow valid comparisons to be made to force plate measures of JH, CT and RSI during countermovement jump and drop jump tasks. The gFlight sensors can therefore be considered a cost-effective, portable measurement system with high concurrent and ecological validity for the objective measurement of jump performance in applied settings.

References

1. Bosco C, Luhtanen P, Komi P V. A simple method for measurement of mechanical power in jumping. *Eur J Appl Physiol Occup Physiol.* 1983;50(2):273–82.
2. Harman EA, Rosenstein MT, Frykman PN, Rosenstein RM, Kraemer WJ. Estimation of Human Power Output from Vertical Jump. *J Strength Cond Res.* 1991;5(3).
3. Markovic G, Dizdar D, Jukic I, Cardinale M. Reliability and Factorial Validity of Squat and

- 1
2
3
4
5
6
7
8
9
10
11
12
13
14
15
16
17
18
19
20
21
22
23
24
25
26
27
28
29
30
31
32
33
34
35
36
37
38
39
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60
- Countermovement Jump Tests. *J Strength Cond Res.* 2004;18(3).
4. Coutts AJ, Slattery KM, Wallace LK. Practical tests for monitoring performance, fatigue and recovery in triathletes. *J Sci Med Sport.* 2007;10(6):372–81.
5. Twist C, Highton J. Monitoring fatigue and recovery in rugby league players. *Int J Sports Physiol Perform.* 2013;8(5):467–74.
6. Glatthorn JF, Gouge S, Nussbaumer S, Stauffacher S, Impellizzeri FM, Maffiuletti NA. Validity and Reliability of Optojump Photoelectric Cells for Estimating Vertical Jump Height. *J Strength Cond Res.* 2011;25(2):556–60.
7. Flanagan EP, Comyns TM. The Use of Contact Time and the Reactive Strength Index to Optimize Fast Stretch-Shortening Cycle Training. *Strength Cond J.* 2008;30(5):32–8.
8. Buckthorpe M, Morris J, Folland JP. Validity of vertical jump measurement devices. *J Sports Sci.* 2012;30(1):63–9.
9. Cronin JB, Hing RD, McNair PJ. Reliability and Validity of a Linear Position Transducer for Measuring Jump Performance. *J Strength Cond Res.* 2004;18(3).
10. Lamkin-Kennard KA, Popovic MB. Integrated systems for obtaining sensory feedback. In: *Biomechatronics.* Academic Press; 2019. p. 99–104.
11. Balsalobre-Fernández C, Glaister M, Lockey RA. The validity and reliability of an iPhone app for measuring vertical jump performance. *J Sports Sci.* 2015;33(15):1574–9.
12. Hojka V, Tufano JJ, Maly T, Stastny P, Jebavy R, Feher J, et al. Concurrent validity of Myotest for assessing explosive strength indicators in countermovement jump. *Acta Gymnica.* 2018;48(3):95–102.
13. Bubanj S, Stankovic R, Bojic I, Boris Đ. Reliability of Myotest tested by a countermovement jump. *Acta Kinesiol.* 2010;2:46–8.
14. Yingling VR, Castro DA, Duong JT, Malpartida FJ, Usher JR, Jenny O. The reliability of vertical jump tests between the Vertec and My Jump phone application. *PeerJ.* 2018;2018(4):e4669.
15. Powell KE, King AC, Buchner DM, Campbell WW, DiPietro L, Erickson KI, et al. The Scientific Foundation for the Physical Activity Guidelines for Americans, 2nd Edition. *J Phys Act Heal.* 2018;16(1):1–11.
16. Jeffreys I. Warm-up revisited: The ramp method of optimizing warm-ups. *Prof Strength Cond.* 2007;6:12–8.
17. Driller M, Tavares F, McMaster D, O'Donnell S. Assessing a smartphone application to measure counter-movement jumps in recreational athletes. *Int J Sports Sci Coach.* 2017;12(5):661–4.
18. Attia A, Dhahbi W, Chaouachi A, Padulo J, Wong DP, Chamari K. Measurement errors when estimating the vertical jump height with flight time using photocell devices: The example of Optojump. *Biol Sport.* 2017;34(1):63–70.

19. Young W, Pryor J, Wilson G. Effect of Instructions on characteristics of Countermovement and Drop Jump Performance. *J Strength Cond Res.* 1995;9(4):232–6.
20. Healy R, Kenny IC, Harrison AJ. Assessing reactive strength measures in jumping and hopping using the optojump™ system. *J Hum Kinet.* 2016;54(1):23–32.
21. Markwick WJ, Bird SP, Tufano JJ, Seitz LB, Haff GG. The Intraday Reliability of the Reactive Strength Index Calculated From a Drop Jump in Professional Men's Basketball. *Int J Sports Physiol Perform.* 2015;10(4):482–8.
22. Hopkins W. Linear models and effect magnitudes for research, clinical and practical applications. *Sportscience.* 2010;14:49–57.
23. Hopkins AG, Marshall SW, Batterham AM, Hanin J. Progressive Statistics for Studies in Sports Medicine and Exercise Science. *Med Sci Sport Exerc.* 2009;41(1):3–12.
24. Hopkins W. Spreadsheets for analysis of validity and reliability. *Sportscience.* 2015;19:36–42.
25. Castagna C, Giovannelli M, Ganzetti M, Ditroilo M, Rocchetti A, Manzi V. Concurrent Validity of Vertical Jump Performance Assessment Systems. *J Strength Cond Res.* 2013;27(3):761–8.
26. Nuzzo JL, Anning JH, Scharfenberg JM. The Reliability of Three Devices Used for Measuring Vertical Jump Height. *J Strength Cond Res.* 2011;25(9).
27. Haynes T, Bishop C, Antrobus M, Brazier J. The validity and reliability of the My Jump 2 app for measuring the reactive strength index and drop jump performance. *J Sports Med Phys Fitness.* 2019;253–8.
28. Choukou M, Laffaye G, Taiar R. Reliability and validity of an accelerometric system for assessing vertical jumping performance. *Biol Sport.* 2014;31.
29. Tenelsen F, Brueckner D, Muehlbauer T, Hagen M. Validity and Reliability of an Electronic Contact Mat for Drop Jump Assessment in Physically Active Adults. *Sports.* 2019;7(5):114.
30. Cormack SJ, Newton RU, McGuigan MR, Doyle TLA. Reliability of Measures Obtained During Single and Repeated Countermovement Jumps. *Int J Sports Physiol Perform.* 2008;3(2):131–44.
31. Hunter JP, Marshall RN, McNair P. Reliability of Biomechanical Variables of Sprint Running. *Med Sci Sport Exerc.* 2004;36(5).